

A Review on Transdermal Drug Delivery System

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ABSTRACT

Transdermal drug delivery, as opposed to conventional topical drug delivery, is the term for drug delivery through the skin to obtain a medicine's systemic effect. Transdermal drug delivery systems (TDDS) are dosage forms in which a significant portion of the drug is transferred into the systemic blood circulation while the remaining portion is delivered to the epidermal and/or dermal tissues of the skin for local therapeutic impact. Currently, 74% of prescriptions are for drugs to be taken orally, yet studies have shown that oral medications frequently have lower efficacy rates due to first-pass metabolism and unstable drug blood levels. The fundamental drawback of transdermal delivery methods is that only drugs with small molecular sizes may be administered using this technique because the skin functions as an extremely effective barrier method. This review article describes the overall introduction of transdermal patches including their types, method of preparation, advantages, disadvantages, the pathway of drug absorption through the skin, marketed preparation, evaluation parameter, and future trends.

I. INTRODUCTION

The term "transdermal patch" often refers to the topical delivery of substances to healthy, intact skin, either for localized therapy of tissues beneath the skin or for systemic delivery. Compared to conventional dosing forms or controlled-release oral systems, transdermal patches have significant benefits. As the largest penetration barrier for drugs is within the stratum corneum, a key drawback of drug delivery patches is that they usually fail to deliver the necessary active component through the skin. Due to the high barrier to penetration across the skin, which is associated primarily with the biological barrier, the use of transdermal distribution to a wider spectrum of medications is constrained. The stratum corneum, the epidermis' top layer. [1], [2]

In contrast to other routes of drug administration, transdermal drug delivery systems avoid a number of problems, including first-pass hepatic metabolism, enzymatic digestion, drug hydrolysis in acidic environments, gastrointestinal irritation, drug fluctuations, adverse effects, therapeutic failure, and the risk of disease transmission. Additional benefits include regulated drug release, cheap cost, and patient compliance. [3]

The first transdermal patch device, which contains scopolamine (hyoscyne) to reduce nausea and vomiting brought on by motion sickness, was introduced in 1979. Since then, it has been a desirable method of medication delivery as well as a difficult field of study. This early technique consisted of a tissue layer supporting a thick layer of adhesive hydrogel that contained the active ingredient. Later, patches included a "reservoir" system with an exterior backing layer, a raised reservoir with the medicine either soluble in an alcohol solution or in solid or gel form, and a polymeric sticky membrane to separate the reservoir from the epidermis and adjust the agent distribution. [2], [4]

However, different transdermal DDS designs have been put forth, from the simplest, which relies on the passive delivery of drugs with little to no permeability enhancement, to the most sophisticated, which enable the delivery of both small and large molecules. In order to enhance the pharmacological effects of drugs, drug carriers (either at the nano- or micro-scale) can be inserted in patches, leading to more effective treatment of such devices. [5]

Transdermal medication delivery devices are used for treating a variety of skin conditions, as well as angina pectoris, pain, quitting smoking, and neurological conditions like Parkinson's disease. This study summarizes the work that has been done in recent years to produce patches with various designs and explore their potential as medication delivery systems. Future prospects and the advantages and disadvantages of

thesystemsthatarenowinusewillbe explored.[5],[6]

Anatomy and physiology of skin:

The skin is the largest organ in the body and has a surface area of about 1.5 to 2 sq. meters in adults and includes glands, hair, and nails. There are two main layers: the epidermis and the dermis.

Epidermis:

The epidermis is the topmost layer of skin and is made up of stratified keratin squamous epithelium, which varies in thickness depending on where the body is located. The palms of the hands and the bottoms of the feet are where it is thickest. The dermis' interstitial fluid, which supplies oxygen and nutrients and drains away as lymph, bathes the different layers of the epidermis, which contains blood vessels or nerve endings.[7]

a) Stratum corneum:

The skin's topmost layer is referred to as this horny layer. When it is roughly 10 μm thick when dry but swells to many times its thickness when wholly hydrated. 10 to 25 dead layers are present. Corneocytes are keratinized cells. Though adaptable and pretty impenetrable. In the stratum corneum, there is the main obstacle to drug entry. An example of how to model the Horny layer's architecture wall-like construction. The keratinized skin in this simulation incorporates lipid, cells that work as protein "bricks," "mortar."

b) Viable epidermis:

This layer, which lies under the stratum corneum, ranges in thickness from 0.06 mm on the eyelids to 0.8 mm on the palms. It is composed of different layers as it moves inward, including the stratum basale, stratum lucidum, stratum granulosum, and stratum spinosum. The epidermis is continuously renewed by cell division in the basal layer, which makes up for the loss of dead Horny cells from the skin's surface. The basal layer's outward-moving cells undergo morphological and histochemical changes as they undergo keratinization to form the stratum corneum's topmost layer.[8]

Three steps are necessary to keep the epidermis healthy:

- 1) The keratinized cell's surface desquamation
- 2) The cell is effectively keratinizing as it approaches the surface.
- 3) Constant cell division in the deeper layers, where freshly created cells are propelled

to the surface.[7]

Dermis:

The dermis is a 3 to 5-mm thick layer made up of a connective tissue matrix that houses nerves, blood vessels, and lymphatic vessels. The control of body temperature relies heavily on the cutaneous blood supply. While removing pollutants and waste, it also gives the skin nutrition and oxygen. Most molecules that penetrate the skin barrier sink in capillaries, which are located 0.2 mm from the skin's surface. Thus, the blood supply maintains a very low dermal concentration of a permeant, and the ensuing concentration gradient across the epidermis is necessary for transdermal penetration.[8]

Hypodermis:

The dermis and epidermis are supported by the hypodermis or subcutaneous fat tissue. Its functions as a place to store fat. This layer aids in temperature regulation, offers nutrients support, and protects mechanically. Principal blood arteries, nerves, and possibly pressure-sensing organs are carried thereto the skin. For transdermal drug administration, the medication must pass through all three of these layers and enter the bloodstream, whereas for topical drug delivery, just stratum corneum penetration is necessary, and the drug should then be retained in the skin layers.[7]

Pathway of drug absorption

through the skin Transfollicular Absorption:

The transfollicular route is the quickest route for a drug to take in order to get to the systemic circulation, which offers a vast region for drug dispersion. The skin has numerous sweat glands, oil glands, hair follicles, and pores that open to the skin's outside surface through their ducts. These ducts provide a continuous channel across the stratum corneum for the transport of medications, although many parameters, such as gland secretion, the composition and volume of secretion, etc., alter the transport of pharmaceuticals through this route. The transfollicular route is the quickest route for a drug to take in order to get to the systemic circulation, which offers a vast region for drug dispersion. Skin has numerous sweat glands, oil glands, hair follicles, and pores that open to the skin's surface.[9]

Transdermal Absorption:

The transdermal drug delivery system works

by allowing drug molecules to diffuse through the epidermal layers of the skin from the drug reservoir in the transdermal patch. As a barrier, the stratum corneum, which is regarded as the rate-limiting membrane in transdermal drug delivery systems, poses a significant impediment. Partitioning into the stratum corneum is the initial step in trans epidermal permeation, after which tissue-to-tissue diffusion occurs. Since the epidermis lacks a direct blood supply, the permeating drug must diffuse across it in order to reach the wet cell mass of the epidermis. The epidermal cell membranes are tightly packed together, and there are no intercellular spaces for ions and polar nonelectrolyte molecules to diffuse through. [10]

Intercellular Route:

Drugs are transported by the continuous lipid matrix in the intercellular route. For two reasons, this approach presents a major challenge. In contrast to the relatively direct course of the transcellular route, the interdigitating nature of corneocytes produces a complex conduit for intercellular drug absorption, which brings to mind the "bricks and mortar" model of the stratum corneum. An area of alternately structured bilayers makes up the intercellular domain. Thus, a medication needs to repeatedly diffuse through aqueous and lipid domains and progressively partition into each. Small, uncharged molecules commonly enter the skin by this pathway, which is widely acknowledged as the most prevalent one. [11]

TYPES OF TRANSDERMAL DRUG DELIVERY SYSTEM

A. Reservoir System:

In this drug system, a drug reservoir is held between the support layer and velocity control membrane. Release from rate-controlled microporous membranes. The drug can be in the form of a solution, suspension, or gel dispersed in a solid polymer matrix in the reservoir section. [12]

B. Matrix System

1) Drug-in-adhesive system-

for the formation of drugs After dispersing the drug in the adhesive polymer, Dispersion of Medicated Polymer Adhesives with Solvents Melt cast or glue (use hot melt adhesive) on an impermeable carrier layer. [11]

2) Matrix-dispersion system

The drug is dispersed in a matrix dispersion system Uniform in a hydrophilic or lipophilic polymer matrix. This containing polymer is then immobilized together with the drug Obstructing base plate in the compartment of the drug impermeable back sheet. The adhesive spreads surrounding instead of applying to the surface of the drug Reservoirs for forming adhesive edge strips. [12]

C) Micro-Reservoir System

This system is a combination of reservoir and matrix dispersion systems. Here the active ingredient is suspended in an aqueous solution. Disperse the solution after dispersing the water-soluble polymer Homogeneous with lipophilic polymer, thousands of Non-leaching microscopic spheres of drug reservoirs. [11]

D) Single-layer drugin adhesive:

This is a type that contains a drug in the adhesive layer. Adhesive layers are not only used to glue different layers together, but they are also responsible for the release of drugs Skin. Adhesive layer is temporarily enclosed by liner and pads. [11]

E) Multi-layer drugin adhesive:

This type is also similar to the single-layer type, but the drug immediately release in layer and other layers control the release together with the adhesive layer. The adhesive layer is responsible for the release of active ingredients. [11]

F) Vapor transdermal patches

Transdermal vapor patches consist of a single layer of adhesive polymer containing vapor-releasing properties. Various steam skin patches are available on the market and used for various purposes. NicoDerm for example CQ is a transdermal nicotine patch that contains essential oils upon release. Helps quit smoking. This product was introduced to the European market in 2007. [3]

Kinetics of Transdermal Permeation: [9]

The main mechanism by which drugs are absorbed Transdermal is the passive diffusion of drugs through the skin in which the drug is absorbed according to concentration gradient due to high drug concentration Resides in the skin or within the skin Drug

molecules diffuse from the reservoir into the system circulation through the skin. drug absorption rate Diffusion by passive diffusion is controlled by Fick's law.

The transmittance Q/dt is given by $Q/dt = Ps(C_d - C_r) \dots (1)$

where C_d is the donor phase concentration, i.e. skin surface and C_r is the drug concentration in the receptor phase. H . Whole body application to the skin traffic jam public relations is the overall permeability and is given by the following formula:

$$Pr = (K_s D_{ss} / h_s) \dots (2)$$

Where K_s is

the partition coefficient of the drug and D_{ss} is the Apparent diffusivity of the drug and h_s is the thickness of the skin. Therefore, the magnetic

permeability P_s can be considered as

K_s , D_{ss} , and h_s (from Equation 2) are Constant under certain conditions. that's why a constant diffusion rate is achieved when $C_d > C_r$. so evaluate The spread Q/dt in Equation 1 can be reduced to $Q/dt = Ps \cdot Disc \dots (3)$

To keep the penetration rate (dQ/dt) constant, C_d The value should remain constant throughout the penetration process through the skin. To keep the medication constant Release rate (R_r) must always be greater than the absorption rate (R_a), i.e. ($R_r > R_a$). Therefore, the concentration of drugs on the skin surface is always given Greater than the saturation solubility of the drug in the skin (C_{es}) i.e.

$C_d > C_{es}$ and maximum skin permeability (dQ/dt) must then $(dQ/dt)_m = Ps \cdot C_e$

Components of transdermal patch:

1. Backing layer

External protection of macromolecular drug reservoirs Provide environment, support, and accept print. Carrier webs must have optimum elasticity and flexibility to Prevent drug diffusion to prevent drug loss. That Must be compatible with polymers, excipients, and drugs ,do not provoke any reaction. It's a forgery of aluminum foil, polyethylene, polyester, polyvinyl chloride, heat seal layer, polyurethane, and cover foam pad.[9]

2) Polymer matrix:

The drug is released from the device below polymer control.[13]

3) Drug

Drug substances are directly attached to the release liner s..[12]

- Drugs need molecular Weight less than about 1000 Daltons.
- Has both lipophilic and hydrophilic phases Required for drug affinity.
- Drug must have a low melting point.
- For a drug to work, Daily doses of a few milligrams should be sufficient.
- A short half-life ($t_{1/2}$) is required. an allergic or irritant reaction to Drugs should not occur.[13]

4) Release liner

It is a reliable and essential packaging material. Peel off the patch while using the patch on the skin. Consists of the non-occlusive base layer (e.g. paper tissue) or occlusive such as polyethylene, PVC.[14]

5) Adhesive

The glue keeps the patches in constant contact Skin. Use your finger to apply it to the skin Pressure should be applied to hold the patch in place longer period. Patch selection criteria are Patch type and design, and adhesive properties. It should be Non-irritating and compatible with other ingredients .The formula is gentle on the skin and can be easily removed. for example. Polyisobutadiene, polyacrylate, silicone adhesive polymer.[9]

6) Permeation enhancers:

Permeation enhancers are used to increase the permeability of the stratum corneum (SC) layer. Drug candidates achieve higher therapeutic levels. Structural components of the stratum corneum, such as proteins Lipids are affected by permeation enhancers. Changes in protein and lipid packaging SC is done by penetration enhancers, thus chemically modifying skin barrier function leading to increased transparency.

Penetration enhancer for TDDS

1. Solvents- Methanol, Ethanol, Dimethyl sulfoxide
2. Anionic Surfactant – Sodium Lauryl Sulfate
3. Nonionic surfactant Pluronic F68, Pluronic F128
4. Essential oils – cardamom oil, cuminoil, lemon oil, menthol (Singh MC et al., 2010) Pressure sensitive adhesive (PSA)[15]

VARIOUS METHODS FOR PREPARATION OF TDDS:

1) Asymmetric TPX Membrane Method:

Using as the backing a polyester sheet (type 1009, 3m) with a concave diameter of 1cm prototype patch could be created for the membrane. The concave membrane is covered by poly (4-methyl-1-pentene)-asymmetric membrane (TPX), which is then affixed with an adhesive.[13] Preparation of asymmetric TPX membranes a dry/wet inversion is used to create them. To prepare polymer solution with dissolved TPX Cyclohexane with non-solvent additive, 60°C. With a gardening knife, the polymer solution Pour into a glass plate at 40°C for 24 hours. Dissolve the cast film at 50°C for 30 minutes. Seconds before melting into a clot Bath (temperature is kept at 25°C). Then you can start removing and drying the membrane Soak [10 minutes in an oven at 50°C]. [13]

2) Mercury Substrate Method:

This approach involves dissolving the needed amount of medication in a solution of polymer and plasticizer. Stirring the aforementioned remedy for a few It takes some time to create a homogeneous dispersion, so after waiting for the last of the air bubbles to disappear, it is poured into a glass ring that is put over the mercury surface in a glass petri dish. By putting an inverted funnel over the petri dish, the pace at which the solvent evaporates can be managed. The films should be kept in a desiccator after drying. [16]

3) Circular Teflon mould method- (Baker and Heller 1989):

As an organic solvent, polymeric solutions in various ratios are utilized. The answer is then split into two halves. The medicine is dissolved in one-half of the calculated amount and in the other half. Two halves are combined once the enhancers at various concentrations have been dissolved. The drug-polymer solution is supplemented with a plasticizer, such as Di-N-butyl phthalate. The entire mixture must be stirred for 12 hours before being placed into a circular Teflon mould. In a laminar flow hood model with an air speed of 0.5 m/s, the moulds must be set upon a flat surface and covered with an inverted funnel to manage solvent vaporization. For 24 hours, the solvent is allowed to evaporate. The dry films must be kept for a further 24 hours at 25.0°C. [12]

4) Glass Substrate Method:

Then keep the polymer solution on one side and let it swell. Add the required amount of

plasticizer and active ingredient solution. Stirred for 10 minutes. Also, for some, it's the page. Eliminate trapped air, then time pour. Clean and dry the Anumbra Petri Plate. solvent rate Evaporation is controlled by inverting the glass funnel Petri dish. After overnight, remove the dried film. Remove and store it in a desiccator. [16]

5) "IPM Membrane method"

- in this method medicine dispersed in a mixture of water and propylene glycol. Contains Carbomer 940 polymer and is stirred for 12 hours with a magnetic stirrer. The variance must be neutralized. Triethanolamine was added to thicken. Buffer pH 7.4 can be used to obtain solution. Gels where the active substance has a very high solubility in aqueous solutions poor. The formed gel is incorporated into the IPM film. [17]

6) By using "The EVAC membranes" method

Manufacture of transdermal targeted drugs system, 1 x Carbopol reservoir gel, polyethylene (PE), Ethylene Vinyl Acetate Copolymer (EVAC) Membrane is Used as a speed control diaphragm. If the drug does not dissolve. Make a gel using water and propylene glycol. medicine is Add Carbopol resin dissolved in propylene glycol. Add to the above solution and neutralize using 5% w/w Sodium hydroxide solution. Put medicine (gel) A backing that covers a designated area. Place the rate-limiting membrane on top of the gel, Edges are heat sealed to prevent leaks device. [12]

7) Aluminium Backed Adhesive Film Method:

Transdermal drug delivery systems can be unstable Matrix for loading >10 mg. The aluminum-coated adhesive film method is suitable. To prepare the same, chloroform is the solvent of choice. Most medicines and glues dissolve in chloroform. The drug is dissolved in chloroform, Add adhesive to the chemical solution, dissolution. Custom-made aluminum formers are lined up. Wrap in aluminum foil and seal the end tightly with cork block. [16]

8) Free film method:-

The free film of cellulose acetate is made by casting on a mercury surface. polymer A solution of 2% w/w should also be prepared in chloroform. The plasticizer is a Concentration of 40% by weight of polymer weight. 5ml Pour the polymer solution into the glass ring, and Placed on the mercury surface of a

glass Petri dish. The evaporation rate of the solvent is to Place the inverted funnel on top of the petri dish. The film Detect formation by observing the mercury surface after complete evaporation of the

solvent dry film organized and stored between leaves and Wax paper until use in a desiccator. [17]

Table no.1-TDDS MARKETED PRODUCTS [18], [19]

Product Name	Drug	Manufacturer	Indication
Alora	Estradiol	TheraTech/Proctol and Gamble	Postmenstrual syndrome
Androderm	Testosterone	TheraTech/GlaxoSmithKline	Hypogonadism in males
Catapres-TTS	Clonidine	Alza/Boehringer Ingelheim	Hypertension
Climaderm	Estradiol	Ethical Holdings/Wyeth-Ayerest	Postmenstrual syndrome
Climara	Estradiol	3M Pharmaceuticals/Berlex Labs	Postmenstrual syndrome
Deponit	Nitroglycerin	Schwarz-Pharma	Angina pectoris
Duragesic	Fentanyl	Alza/Janssen Pharmaceutica	Moderate/severe pain
Estraderm	Estradiol	Alza/Novartis	Postmenstrual syndrome
Fematrix	Estrogen	Ethical Holdings/Solvay Healthcare Ltd.	Postmenstrual syndrome
FemPatch	Estradiol	Parke-Davis	Postmenstrual syndrome
Habitraol	Nicotine	Novartis	Smoking cessation
Minitran	Nitroglycerin	3M Pharmaceuticals	Angina pectoris
Nicoderm	Nicotine	Alza/GlaxoSmithKline	Smoking cessation
Transderm-Scop	Scopolamine	Novartis Consumer Health (Parsippany, NJ, USA)	Motion sickness
Neupro	Rotigotine	Schwarz Pharma (Mequon, WI, USA)	Parkinson's disease
Exelon	Rivastigmine	Novartis	Dementia

Application of transdermal patch [17]

- 1) Transdermal nicotine patches to be released Controlled dose of nicotine to help quit smoking smoke a cigarette
- 2) Nitroglycerin patch sometimes it was prescribed for the treatment of angina pectoris.
- 3) clonidine, anti-hypertensives and ketoprofen, non-steroidal anti-inflammatory drugs It is available in the form of a transdermal patch.
- 4) MAOI selegiline transdermal absorption type was ingested First means of transdermal administration of antidepressants.
- 5) Transdermal drug for attention deficit hyperactivity disorder (ADHD).

ADVANTAGES [8],[13],[16]

1. Prevent first-pass gastrointestinal and hepatic metabolism.
2. Makesure the control absorption is constant.
3. lessens negative effects
4. Limit exposure to harmful metabolites.
5. Increased patient compliance because multiple dosing is no longer necessary.

6. Increase the effectiveness of therapy.
7. Simple to use and take away.
8. Painless and minimally invasive
9. Self-governance.
10. Functions well for medications with brief biologic half-lives and restricted therapeutic windows.
11. Simple to stop dosing in the event of a bad reaction.
12. Repeated sustain release.
13. Transdermal drug delivery makes it possible to avoid gastrointestinal absorption and its associated risks of enzymatic and pH-related deactivation.
14. Refraining from first-pass metabolism.
15. Drugs requiring relatively constant plasma levels are excellent candidates for transdermal drug delivery because the absence of peaks in plasma concentration can lower the risk of side effects.
- In place of the oral route.
17. The patch also allows for continuous dosing rather than the peaks and valleys in medication level common with orally administered medications.
18. The ability to quickly stop the effects of a drug by removing a patch, as well as

quick notifications of medication in an emergency

Limitations

1. Drugs requiring high blood levels cannot be administered.
2. Adrugorits formulation may irritate and sensitise the skin.
3. The skin's ability to act as a barrier varies from one site to another on the same individual, from person to person, and with age.
4. Not feasible if the drug is heavily metabolised in the skin and if the molecular size is too large to allow the molecule to diffuse through the skin.
5. Might lead to an allergic reaction.
6. Consistency over time is challenging.
7. Ionic medications cannot be delivered using a transdermal drug delivery system.
8. High drug levels in the blood cannot be achieved.
9. It is unable to develop for drugs with large molecular weights.
10. It is unable to deliver medication pulse-by-pulse.
11. It cannot develop if the medication or formulation irritates the skin.
12. A possible local inflammatory reaction at the application site.
13. Might lead to an allergic reaction.

Tableno.2-PolymersUsedIn TransdermalPatch

Sr.No.	Polymers	Reference
1	EC	[1]
2	HPMC K4M/K100/PVP	[20]
3	PVA	[21]
4	Silicone Elastomer	[22]
5	HPMC/Chitosan	[23]
6	Carbopol	[24]
7	HPMC	[25]
8	Eudragit,PVP	[26]
9	PG	[27]
10	PEG	[28]

EC- Ethyl Cellulose
 PVA-Polyvinyl Alcohol
 PVP-Polyvinyl Pyrrolidone
 HPMC- Hydroxypropyl methylcellulose
 PG- Propylene Glycol
 PEG-Polyethyleneglycol

Medicine in adhesive technology Systems is Recommended for Passive Transdermal Delivery has two areas of formulation research Focus on adhesives and secondary materials. glue Research Focuses on Adhesive Customization Improves adhesion to the skin when worn duration, improves drug stability and solubility,

ADVANCED DEVELOPMENT IN TDDS:

Decreases latency, and increases speed delivery. Free size glue None can absorb all drugs and formulation chemistry, adjustment adhesive chemistry allows percutaneous absorption Formulator for optimizing the performance of transdermal patch. Rich research fields in the last 10-15 years [29]

Concentration Development of transdermal absorption technology Increase using mechanical energy drug flow across the skin by changing either the Skin barrier (mainly stratum corneum) or increased energy of drug molecules. This so-called "Active" transdermal techniques include: Iontophoresis uses low-voltage current to power the charged drug through the skin.

Easy to use electroporation high voltage electric impulse Creates temporary watery pores skin. Sonophoresis (low frequencies that interfere with ultrasonic energy stratum corneum) and heat energy (

Increases skin permeability and weight gain energy of drug molecule).

Also, cast magnetic energy was magnetophoresis studied as a means to increase its Drug flow across the skin. [18]

LIMITATIONS FOR SELECTION OF TDDS:

Not all types of drugs can be administered this way. Root; the drug should have some desirable physical properties. chemical properties.

- Not suitable for pharmaceuticals requiring high plasma levels.
- Not suitable for agents that cause skin irritation or contact dermatitis.
- Not suitable for high molecular weight drugs.
- Not suitable for drugs metabolized during this time passage through the skin. Larger ones cannot use the transdermal route. Since the skin is a very effective barrier, various drugs for drug penetration. Only possible at low doses managed. [16]
- Medications that require high blood levels cannot be administered
- Medication formulations may cause irritation or sensitization. [6]
- Drugs metabolized during this time are not suitable to pass through the skin. This method. [13]

Evaluation Parameters of Transdermal Patch.

1) **Folding Endurance:**- strip of a specific area

(2 cm*2 cm) was cut evenly and repeatedly folded at the same place till it broke. The number of times the film was folded at the same place without breaking gave the value of the folding endurance. [20]

2) **Tensile Strength:**- Using a tensiometer, the patch's tensile strength was assessed. There are two load cell grips in it. The upper one could be removed, but the lower one was fixed. Between these cell grips, 2 x 2 cm film strips were fastened, and force was gradually exerted. [20]

3) **Percentage Elongation Break Test:**- The length right prior to the breakpoint was used to determine the percentage elongation break, which was then calculated using the formula below. $\text{Elongation percentage} = \frac{(L1 - L2)}{L2} \times 100$, where L1 is the final length of each strip, and L2 is the initial length of each strip. [20]

4) **Thickness:**- Using a digital micrometer, the thickness of the drug-loaded patch is measured at several sites, and the average thickness and standard deviation is calculated. At various spots along the transdermal film, the thickness is measured using a traveling microscopical gauge, screw gauge, or micrometer. [20]

5) **Drug Content:**- In 100 mL of methanol, a predetermined patch area (2 cm x 2 cm) was dissolved, and the mixture was continually shaken for 24 hours. Next, the entire solution was ultrasonically sonicated for 15 minutes. Following filtering, the drug's concentration was evaluated by spectrophotometric estimation at a wavelength of 281 nm.

6) **Percentage Moisture Content:**- For 24 hours, individually weighed patches are stored in desiccators with fused calcium chloride at room temperature. The patches must be weighed and measured 24 hours later. A formula is used to determine the percentage moisture content.

Percentage moisture content: $-\frac{(\text{Initial weight} - \text{Final weight})}{\text{Final weight}} \times 100$ [20]

7) **Percentage Moisture Uptake:**- The weighed films were kept in a desiccator at room temperature for 24 h containing a saturated solution of potassium chloride in order to maintain 84% RH. After 24 h, the films were reweighed, and determine the percentage moisture uptake from the below-

mentioned formula:

Percentage moisture uptake = $\frac{\text{Final weight} - \text{Initial weight}}{\text{Initial weight}} \times 100$...[20]

8) Weight Of Patch:-

Each patch from a specific formulation is weighed separately on a digital balance to determine the standard deviation.[18]

9) **Stability studies:** In accordance with the ICH recommendations, stability studies must be carried out by holding TDDS samples at 40°F and 75 RH for six months. The samples are taken at 0, 30, 60, 90, and 180 days and properly analysed for the presence of drugs.[30]

10) **Percentage Moisture Loss:** The prepared patches are weighed separately and maintained in desiccators with anhydrous calcium chloride at room temperature for 24 hours. The patches are weighed every seven days after the first 24 hours until a steady weight is achieved.

Moisture loss is calculated by using the following formulae:

Percentage moisture loss = $\frac{(\text{Initial weight} - \text{final weight})}{\text{initial wt}} \times 100$. [31]

11) **In-vitro skin permeation studies:** Using diffusion cell equipment, it is possible to measure how well a drug penetrates the skin. In the experiment, pig skin is primarily employed and mounted between the donor and receptor compartments. Comparing the cumulative permeation profiles of skin that has been microneedled and untreated skin.[32]

12) **Skin irritation evaluation:** Albino rabbits (N = 15) were divided into 5 animals and a skin irritation test (9) was conducted. Groups, 3 rabbits in each group. Group, I marked as control (no treatment), Group II was also pasted with commercially available adhesive tape (Nichi pore Surgical Tape, Japan), considered a control group. Apply DXIBN transdermal patch to bare skin Group III and Group IV blank patch (no drug) Standard stimulant was formalin Applied to Group V animals, the experiment was conducted over 7 days. Group (reapply the

new patch to the same location every 24 hours for 7 consecutive days) and application sites were similarly rated on a visual rating.[21]

FUTURE TRENDS IN TDDS

In the future, the transdermal route is the most preferred Medication management by improving patient compliance, Dosage control, reduction of dosing frequency, etc. 2 Decades ago, nicotine patches were developed for smoking Settings for transdermal use and many wins Very popularly. After that, many drugs were prescribed Transdermal patches such as nitroglycerin and estradiol for angina pectoris Fentanyl for opioid deficiency, fentanyl for pain, etc. The patent term encouraged researchers to Formulate drugs with new acceptable dosages to the application form. The popularity of transdermal delivery systems Moreover, it is continuously increasing. Improved design and technology. leadership A pharmaceutical company is working on its TDDS, Many techniques for the transdermal route are Working on these technologies with these companies' successful performance. new distribution systems such as Liposomes, niosomes, nanoparticles, microspheres, etc. Microemulsions are used in the formulation of TDDS. Increases solubility with improved absorption of Insoluble drugs. Other infiltration techniques Other improvements have also been made. B. use mechanical energy that increases drug flux across the skin by altering or increasing the physiology of the skin Velocity of drug molecules. electrophoresis, Iontophoresis, sonophoresis, and magnetophoresis are Other techniques studied for Improved drug delivery across the skin Drugs with molecular weight and insoluble drugs . The current scenario has emerged as the safest and safest skin Acceptable route of drug delivery to the system Circulatory, anti-oral route [9]

II. DISCUSSION

This article provides valuable information and details of the evaluation process on transdermal drug delivery systems as a ready reference for researchers working with TDDS. The foregoing indicates that TDDS has great potential to exploit both hydrophobic and hydrophilic drugs into promising deliverable drugs. Optimizing this drug delivery system requires a better understanding

of the biological interactions and different mechanisms of the polymers.

The transdermal route of drug delivery is safe and effective compared to other routes of administration. Many drugs are formulated with TDDS, such as hormone therapy, a wide range of pain relievers, heart disease drugs to avoid GI action and first-pass metabolism. Due to several advantages and popularity of transdermal drug delivery, which attract the attention of researchers and intend to introduce many new drugs in transdermal form. The main function of the skin is to protect the internal organs, but transdermal administration of drugs can alter the physiology of the skin, so this should be considered when designing a transdermal delivery system that alters the natural functions of the skin at least possible. A better understanding of the physiology and anatomy of the skin will help us move forward in this field.

However, the design and optimization of transdermal delivery require excellent knowledge and understanding of the interactions between different polymers and skin components.

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